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<b>(21) International Application Number:</b> PCT/SE97/01901 <b>(22) International Filing Date:</b> 12 November 1997 (12.11.97)  <b>(30) Priority Data:</b> 9604124-9                      12 November 1996 (12.11.96)      SE 60/031,723                      25 November 1996 (25.11.96)      US  <b>(71) Applicant (for all designated States except US):</b> PHARMACIA & UPJOHN AB [SE/SE]; S-112 87 Stockholm (SE).  <b>(72) Inventors; and</b> <b>(75) Inventors/Applicants (for US only):</b> GREN, Torkel [SE/SE]; Funbo, Skogsängen, S-755 97 Uppsala (SE). NYSTRÖM, Christer [SE/SE]; Holmvägen 22, S-756 51 Uppsala (SE).  <b>(74) Agents:</b> WAHLSTRÖM, Christer et al.; Pharmacia & Upjohn AB, S-112 87 Stockholm (SE).		<b>(81) Designated States:</b> AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, DE, DK, EE, ES, FI, GB, GE, HU, IL, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, TJ, TM, TR, TT, UA, UG, US, UZ, VN, ARIPO patent (GH, KE, LS, MW, SD, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG).  <b>Published</b> <i>With international search report.</i>
<b>(54) Title:</b> COMPACT MEMBER COMPRISING A PLURALITY OF POROUS CELLULOSE MATRICES, (PCMs), METHOD OF MANUFACTURING AND USE THEREOF  <b>(57) Abstract</b>  The invention relates to a compact member comprising a plurality of porous cellulose matrices (PCMs), and providing extended release of an active compound located in the pores of said PCMs together with a release-modifying agent. The friability of the compact member is less than 2.1%, and the disintegration time <i>in vitro</i> of said compact member is less than 240 minutes. The compact member is manufactured by exposing a plurality of PCMs to an active compound and a release-modifying agent, in optional sequence or mixture, for a time sufficient for said active compound and release-modifying agent to fill the pores in said PCMs to a preselected level. The PCMs are subsequently compacted to a desired shape. The invention further relates to use of the compact members for administration of a drug.		

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COMPACT MEMBER COMPRISING A PLURALITY OF POROUS CELLULOSE MATRICES, (PCMs), METHOD OF MANUFACTURING AND USE THEREOF

### TECHNICAL FIELD OF THE INVENTION

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The present invention relates to a compact member having extended release of an active compound. In particular it relates to a tablet based on multiple-units made of porous cellulose matrices (PCMs), and having the property of at the same time being easily handled without being damaged, and having an adequate rate of disintegration.

10 The release rate of the active compound is controllable.

### BACKGROUND OF THE INVENTION AND PRIOR ART

15 Simple incorporation of drugs into PCMs (without coating) may retard the drug release but usually not to an extent sufficient for extended release purposes, and has therefore not been commercially feasible.

20 Extended release of an active compound, e.g. a drug, is possible to achieve by providing drug-loaded porous beads with a coating, such as a release-controlling, water permeable film or membrane. This technique has been extensively used heretofore in the art. In the process of forming such films or membranes organic solvents are often needed, which from both economic and environmental point of view is undesirable.

25 Multiple-unit (MU) preparations containing a plurality of pellets have been used as carriers of drugs previously. The use of MU drug preparations is considered to promote good absorption properties since they are dispersed over a large area in the gastrointestinal (GI) tract. Furthermore, they are considered to have a lower transit rate especially in the colon compared to matrix tablets. In addition, MU preparations are preferable to single unit preparations, since they may be divided into smaller portions all having the same release and absorption properties which will give greater flexibility in selection of the dose size. Also, MU preparations will facilitate administration of the  
30 drug to patients having problems to swallow and will considerably reduce the risk of dose dumping.

Extended release multiple-units (MUs), based on porous matrices of the type mentioned above, as carriers of drugs have commonly been filled in hard gelatine capsules. However, there is an increasing interest in the compaction of extended release multiple-units into disintegrating tablets. The reason for this is the advantages of tablets over the above mentioned capsules, such as more rational production, higher dose accuracy and lower risk of tampering. Unfortunately the release rate is often affected by compaction. The release rate may increase due to crushing, formation of cracks in the release-controlling coating etc., or decrease due to complete or partial failure of tablets to disintegrate. Tablets made of coated multiple-units with intact or nearly intact release rate by the use of relatively large amounts of excipients have been reported. The function of the added excipients may be to protect the film by absorbing energy during compaction or to act as disintegrants.

PCMs may e.g. be prepared by a wet or a dry method as disclosed in International Patent Applications WO-A-91/18590 and WO-A-94/23703, respectively, both assigned to Pharmacia & Upjohn AB of Sweden. The preparation of PCMs does not form part of the invention, and will not be specifically discussed herein. Instead, the said patent applications are incorporated by reference. PCMs are normally small spherical particles, so-called pellets, with a diameter in the range of from about 0.5 up to about 1.5 mm, suitably with a diameter of about 1 mm.

Other methods for making pellets of cellulose, optionally incorporating one or more additional substances, e.g. lipids, could be extrusion/spheronization, "layering", melt-pelletization and spray-cooling.

Extrusion/spheronization is performed by pressing a moistured powder mass through a metal sheet wherein a plurality of holes has been made. The mass thereby forms spaghetti-like threads. These threads are transferred to a horizontally rotating plate, where they are broken to pieces and formed to spheres which subsequently are allowed to dry.

In "layering", powder and liquid are added to small seeds (commonly sugar), having been rotated in a so-called pan or the like. Layer by layer, larger spheres are built.

In melt-pelletization, spheres can be formed in a Teflon®-coated mixer when part of the powder melts.

In spray-cooling a melt is comminuted into small droplets that solidify and form small spheres.

5       The above methods are part of the prior art and the skilled man will be able to manufacture beads according to any of said routes by virtue of his ordinary skill.

Porous cellulose matrices (PCMs) have been shown to be potential multiple-unit (MU) drug carriers (Davidson et al., "Porous cellulose matrices - a novel excipient for the formulation of solid dosage forms", Int. J. Pharm. 100 (1993) 49-54).

10       A possible method to modify the drug release rate from non-compacted PCMs is by incorporating release-modifying substances together with the drug into the pores of the cellulose matrix, as disclosed in WO-A-91/18590.

If thermoplastic materials could be used as release modifiers, the incorporation could be done by making use of such materials in a molten state. It might then be  
15       possible that the process be carried out without excessive energy input or organic solvents. Especially if the drug could be incorporated by suspending it in or otherwise mix it with the melted release modifier, this process could be very cost effective.

Non-compacted PCMs have been shown to extend the release of paracetamol incorporated together with lipids in the matrix pores. This type of spherical extended  
20       release pellets could be produced very cost effectively with low energy consumption and without any organic solvents. Another possible advantage of this type of system is that drug release from matrix pellets of this type may be less sensitive to compression than pellets coated with a thin membrane. It also seems reasonable that the disintegrating effect of cellulose could be advantageous when trying to compact PCMs  
25       into disinte-grating multiple-unit tablets.

As mentioned above, MUs are commonly delivered in doses contained in hard gelatine capsules. It would be desirable to be able to manufacture tablets by compression of MUs, because manufacture would thereby become more cost effective, tablets would be more easily divided in subdoses etc. However, MUs are difficult to  
30       make into tablets by compression since

1) tablets made from MUs do not easily disintegrate upon oral administration, and

2) the MUs are easily crushed or damaged during the compaction process, having as a consequence that the release rate is substantially increased.

In order to avoid the above problems the prior art teaches addition of substantial amounts of various additives, located between the particles. Such measures add to the complexity and cost of the manufacturing process, apart from introducing unnecessary chemicals into the medicaments.

### SUMMARY OF THE INVENTION

It is therefore an object of the invention to provide compact members (tablets) having extended release of an active compound, said compact members having the properties of

- 1) being easy to handle without said members being damaged; and
- 2) rapidly disintegrating *in-vivo* (in the gastrointestinal tract) e.g. when administered orally.

In addition, the above object should be achieved without having to incorporate large amounts of additives in the compact members.

This object is achieved in one aspect of the invention with a compact member comprising a plurality of PCMs, and providing extended release of an active compound contained therein, as claimed in claim 1.

The advantage of the compact member of the present invention is thus the combination of

- 1) it being easy to handle in industrial processes, such as packaging etc., by virtue of its low friability, and
- 2) disintegration times suitable for its intended purpose.

It is a further advantage of the present invention, that the compact members can be given an *in-vitro* dissolution rate which is essentially the same as that exhibited by the uncompacted pellets of which the compact member consist. This means that the amount of drug released does not deviate more than  $\pm 50\%$  of the total amount of drug in the compact member, at any time.



The compact member suitably contains talc, as claimed in claim 6. The release rate may be controlled by varying the talc content. Thereby, the release rate of the active compound can be practically equal to the release rate of free PCMs.

Especially it is suited for use in its preferred embodiment as a tablet containing a drug, as claimed in claim 12.

In another aspect of the invention there is provided a method of manufacturing tablets having the desired properties. This is achieved by the method as defined in claim 14.

In yet another aspect of the invention there is provided use of a compact member according to the present invention for administration of a drug, as defined in claim 20.

The invention will become more fully understood from the following illustrative description of preferred embodiments thereof, by way of non-limiting examples, and with reference to the appended drawing figures.

15

#### BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1 is a graph showing radial tensile strength for tablets according to the invention (filled circles) and tablets of empty PCMs (open squares) as a function of compaction pressure;

20 Fig. 2 is a graph showing disintegration time for tablets according to the invention as a function of compaction pressure;

Fig. 3 is a graph showing release of drug from pellets not according to the invention as a function of time for different lipid compositions;

25 Fig. 4 is a graph showing release of drug from tablets according to the invention as a function of time at two different compaction pressures using two *in-vitro* dissolution methods;

Fig. 5 is a graph showing release of drug for tablets according to the invention as a function of time at five different compaction pressures and for uncompacted pellets;

30 Fig. 6 is a graph showing the effect of talc on release of drug of a tablet according to the invention (tablet of granules and 5 % (w/w) talc (open triangles), tablets without any talc (filled circles)) and uncompressed granules as a reference (X).

### DETAILED DESCRIPTION OF THE INVENTION

Drug release from PCMs has, as mentioned above, been shown to be possible to  
5 extend over at least 16 hours by incorporating release modifiers together with the drug  
into the pores in the cellulose matrix. The rate of release could be adjusted by varying  
the release modifier composition, drug concentration and particle size of the PCMs. The  
release seems to be controlled by diffusion from the matrix but is also affected by the  
distribution of drug in the matrices and an increase of porosity due to erosion of matrix  
10 material and pores formed by the swelling of cellulose. The incorporation of drug and  
release modifier could be performed simultaneously by dispersing a micronized drug  
into the molten release modifiers. Hence, an extended release multiple-unit preparation  
may be prepared from PCMs with a simple, solvent-free, one-step process.

Materials suitable as release-modifying agents are characterized by exhibiting a  
15 low melting point, a low viscosity above the melting point and a low solubility in water.  
The material is suitably only slightly soluble in water and preferably insoluble in water.

Lipids may be suitable as release modifiers for incorporation into PCMs, since  
they are often low-melting, non-toxic, relatively inexpensive and there is a broad range  
of lipids with different physico-chemical properties.

20 Lipids may be classified on the basis of their different interaction with water into  
non-polar lipids (e.g. aliphatic hydrocarbons) and polar lipids. The polar lipids could be  
further subdivided into different classes: I) insoluble nonswelling amphiphilic lipids, II)  
insoluble swelling amphiphilic lipids and III) soluble amphiphilic lipids, where the  
solubility refers to water as a medium.

25 The release rate from lipophilic matrices can often be controlled by the use of a  
mixture of a nonpolar and a polar lipid or of two polar lipids from different classes.

There is no universal definition of "lipid". Lipids are sometimes defined as  
naturally occurring fats, oils and waxes. However, here the word lipid is used in a  
broader sense covering also e.g. aliphatic hydrocarbons and fatty alcohols. Examples of  
30 lipids which have been used as meltable excipients are fatty acids, e.g. stearic acid, long  
chain alcohols, e.g. cetostearyl alcohol, naturally occurring and synthetic waxes,



glyceryl esters of fatty acids, e.g. glyceryl monostearate, glyceryl distearate, or glyceryl tristearate, aliphatic hydrocarbons, e.g. hard paraffin, polyglycerol esters of fatty acids, and any mixture thereof.

In the present invention, it is advantageous to use a release-modifying agent, preferably a lipid, with a melting point in the range of from about 10°C up to about 200°C, suitably from 20°C up to 150°C, and preferably 30°C up to 100°C.

Prior to compaction, small amounts of additives may be added to the PCMs to give the resulting compact members specific properties as regards release rate, tensile strength etc. Thus, the compact members may contain up to about 10 %, and preferably up to 5 % by weight of talc. Also, the compact members may contain up to about 5 %, suitably up to about 1 %, and preferably up to 0.5 % by weight of a lubricant. Suitably, use is made of magnesium stearate, which is a conventional and economic choice.

In the present invention, the PCMs can be made from a wide variety of cellulose raw materials. Suitably, the cellulose raw material is substantially pure, preferably of a pharmaceutical purity grade. It is also conceivable to use one or more chemically modified derivatives of cellulose as raw material, such as carboxy methylcellulose (CMC), alkylcelluloses, e.g. methylcellulose or ethylcellulose, hydroxypropylcellulose (HPC) or alkyl hydroxyalkyl celluloses, e.g. ethyl hydroxyethylcellulose (EHEC), optionally in any mixture with cellulose.

In manufacturing of the compact members according to the present method, the release-modifying agent is incorporated in the pores of the PCMs by any method suitable for the release-modifying agent at issue. For example with lipids, a melt process would be preferable, i.e. the lipid would be melted before incorporation.

The active compounds contained in the compact members of the present invention, are preferably drugs (pharmaceuticals). The present invention is suitable for hydrophilic drugs, i.e. drugs soluble in water or aqueous solutions. Furthermore, the present invention is particularly useful for drugs exhibiting a biological half-life of less than about 20 hours, since extended release of drugs with a longer biological half-life is normally not necessary. The present invention is preferably used for drugs exhibiting a biological half-life of less than 15 hours, and more preferably less than 10 hours.

It should be recognized that the active compound to be incorporated in the compact members of the present invention may be any of a number of different compounds for different uses apart from drugs, e.g. fertilizers, pesticides, herbicides etc.

The compact members of the present invention may contain up to about 50 % by weight of the active compound, suitably up to 10 %, and preferably up to 2.5 % by weight of the active compound.

In manufacturing of the compact members according to the present method, the PCMs can be exposed to the active compound and release-modifying agent in optional order, or preferably simultaneously, after premixing of the active compound and release-modifying agent. The active compound and release-modifying agent can be dry mixed, as disclosed in Example 1 of the present specification. Other types of mixing are conceivable, and for the purpose of this invention, the term mixing would encompass any form of dispersing, suspending, emulsifying etc. which reasonably homogeneously would distribute the active compound in a release-modifying agent.

In order not to obtain unacceptable agglomeration of individual PCMs because of an excess of active compound and release-modifying agent present, the amount of active compound and release-modifying agent necessary to fill the pores to a preselected level for a given batch, is calculated from the densities of the active compound and release-modifying agent and the known pore volume for a given amount of PCMs. The porosity of pure PCMs can be calculated from pellet density data measured by mercury porosimetry and from apparent density data obtained by helium pycnometry. In the present invention, it is suitable that the pores are filled with the active compound and release-modifying agent to at least about 50% of the pore volume, preferably at least 70%, and more preferably at least 80% of the pore volume, before compacting the PCMs.

In manufacturing of the compact members according to the present method, the PCMs comprising an active compound and a release-modifying agent are compacted to a desired shape. Examples of desired shapes of compact members are cylindrical, cylindrical with rounded upper and lower surfaces, cubical and essentially spherical.

In manufacturing of the compact members according to the present method, the pressure in the compacting step is suitably less than about 500 MPa, preferably in the

range of from 10 up to 200 MPa, and more preferably in the range of from 50 up to 150 MPa.

From a medical point of view it is desirable that compact members, such as tablets, exhibit disintegration times *in-vitro* of less than about 240 minutes. The disintegration time *in-vitro* is suitably less than 90 minutes, and preferably less than 60 minutes.

Radial tensile strength is an important property for the compact members of the invention, since the radial tensile strength is a measure of the cohesive properties of the compact members, e.g. tablets. The radial tensile strength of the compact member of the present invention can be higher than about 0.1 MPa, suitably higher than 0.3 MPa, and preferably higher than 0.5 MPa.

### EXPERIMENTAL

The following Examples are provided for purposes of illustration only and are not to be construed as in any way limiting the scope of the present invention, which is defined by the appended claims.

The percentages and parts are per weight, unless otherwise stated.

#### Example 1 (not according to the invention)

A multiple-unit extended release matrix preparation, was prepared by the incorporation of a hydrophilic drug (Paracetamol; Hoechst, Germany) and lipophilic release modifiers (Cetanol; Bionord AB, Sweden, and hard paraffin; MB Sveda, Sweden) into porous cellulose matrices (PCMs).

The PCMs were made according to the method disclosed in WO-A-94/23703. The drug was micronized and dry mixed with a lipid, using a mortar and a pestle. The drug and lipid mixture was then heated on a water bath and the drug was thereby dispersed substantially homogeneously in the molten lipid. PCMs were added during stirring. It is also conceivable to add the drug to the molten lipid, or vice versa. The mixtures were allowed to cool during stirring. The size fractions 0.5 - 0.71, 0.71 - 1.2 and 1.2 - 1.4 mm were obtained by sieving. Two pellets with no cellulose were also prepared for comparison. The various formulations are shown in Table 1.

TABLE 1

Prepared pellets and results from linear regression of  $\ln(\text{released drug})$  vs  $\ln(\text{time})$  for <60% drug released for studied pellets. Lipid concentration is 43 % (w/w)

5 unless otherwise indicated.

	Lipid composition. (paraffin:cetanol) (% w/w)	Paracetamol content (% w/w)	Particle size (mm)	Drug particle size ( $\mu\text{m}$ )
10	1:0	2.5	0.7-1.2	2.2
	1:1	2.5	0.7-1.2	2.2
	1:2	2.5	0.7-1.2	2.2
	1:3	2.5	0.7-1.2	2.2
15	0:1	2.5	0.7-1.2	2.2
	1:2 (40% lipid)	2.5	0.7-1.2	2.2
	1:2 (37% lipid)	2.5	0.7-1.2	2.2
	1:2	2.5	0.5-0.7	2.2
	1:2	2.5	1.2-1.4	2.2
20	1:2	2.5	0.7-1.2	3.4
	1:2	2.5	0.7-1.2	8.4
	1:2	1	0.7-1.2	2.2
	1:2	5	0.7-1.2	2.2

25 The amounts of drug incorporated into PCMs were assayed spectrophotometrically after extraction in ethanol (95%).

The release rates were determined according to USP method I (basket) in distilled water, at 37°C, 100 rpm. The amount released was detected spectrophotometrically ( $\lambda=244$  nm). The amount of pellets was chosen in order to maintain sink condition during the entire release measurement and to get optimal analytical sensitivity. The results are shown in Fig. 3 as release of drug vs time for PCMs loaded

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with various lipid compositions. In Fig. 3 filled squares represent PCM and pure hard paraffin, filled triangles represent PCM and 1:1 of hard paraffin:cetanol, filled circles represent PCM and 1:2 of hard paraffin:cetanol, empty triangles represent PCM and 1:3 of hard paraffin:cetanol, empty squares represent PCM and pure cetanol, and empty  
5 circles represent reference pellets without cellulose matrix, i.e. pure lipid.

As can be seen in the figure, the *in-vitro* drug release could be extended over at least 16 hours. The release rate could be controlled by varying the ratio of cetanol to paraffin.

#### 10 Example 2 (according to the invention)

The possibility to compact PCMs into disintegrating extended release multiple-unit tablets was studied using a hydrophilic drug and lipophilic release modifiers.

Paracetamol (Hoechst, Germany) was chosen as a model drug substance since it is relatively stable and non-toxic and since it has been used in earlier studies.

15 Cetanol (Bionord AB, Sweden) and hard paraffin (MB Sveda, Sweden) was used as release-modifying lipids.

Magnesium stearate (Kebo, Sweden) was used as model lubricant.

Anhydrous silicon dioxide (Aerosil, Degussa AG, Germany) and talc (Kebo, Sweden) were used as anti-adherents.

20 PCMs were manufactured from cellulose using a special process involving mechanical treatment in the presence of water (WO 94/23703). The size fraction 0.71-1.17 mm was obtained by sieving.

Paracetamol and drug-and-lipid mixtures were incorporated into PCMs by the melting procedure as described in Example 1. The composition used contains 54 %  
25 (w/w) cellulose, 43 % (w/w) lipid (cetanol: paraffin 2:1) and 2.5 % (w/w) paracetamol. The loading was performed in subbatches of 150 g. Five subbatches were then poured into a polyethylene bag and mixed by hand shaking.

The porosity of pure PCMs was determined to be 54%. The porosity was calculated from pellet density data measured by mercury porosimetry and from apparent  
30 density data obtained by helium pycnometry.

Some of the drug-and-lipid loaded PCMs were mixed, for 60 minutes, with magnesium stearate, talc and/or anhydrous silicon dioxide in a Turbula Mixer (2 liters, W. A. Bachofen, Switzerland). The batch size of the mixtures was 50 - 100 g.

5 All materials were stored for no less than 48 hours at 40 % relative humidity and room temperature (20-25°C) before compaction. Loaded and empty PCMs were compressed to tablets, at 12 ( $\pm 1$ ), 20 ( $\pm 1$ ), 35 ( $\pm 2$ ), 50 ( $\pm 2$ ), 75 ( $\pm 2$ ), 100 ( $\pm 5$ ) and 200 ( $\pm 5$ ) MPa in a single punch press (Korsch EKO, Korsch, Germany). Flat faced punches with a diameter of 11.3 mm were used. The shortest distance between the punches was set to 3 mm. The particles for each tablet were weighed and poured manually into the  
10 die. A suspension of 1 % magnesium stearate in ethanol (95 %) was used as an external lubricant. The tablets were kept at 40 % relative humidity and room temperature (20-25°C) for at least 48 hours, before characterization.

#### Tensile Strength

15 The diametrical crushing force was measured in a tablet hardness tester (C 50, Holland Ltd., UK). Radial tensile strength was calculated from diametrical compression data according to the method by Fell and Newton (J. Pharm. Pharmacol., 20 (1968) 652-659). The results are shown in Table 2a for 12 MPa and 200 MPa pressures, respectively. The results are shown also in Fig. 1 which shows radial tensile strength vs. com-  
20 paction pressure for tablets of PCMs with incorporated drug and lipids and unloaded PCMs. In Fig. 1, filled circles represent PCMs loaded with drug and lipid, and squares represent unloaded PCMs.



TABLE 2A

Tensile strengths for pellets compressed at 12 and 200 MPa, respectively, with and without some additives.

5	Additives	Radial tensile strength (MPa)	
		Compressed at 12 MPa	Compressed at 200 MPa
	No additives	0.16	0.63
	1% Mg stearate	0.14	0.64
10	5% talc	0.11	0.49
	5% colloidal silicon dioxide	0.094	0.53
	5% colloidal silicon dioxide and 1%		
15	magnesium stearate	0.064	0.68

With reference to Fig. 1, surprisingly it was found that the incorporation of drug and lipid increases the compactability of the PCMs at low pressures, so that coherent tablets are obtained already at 12 MPa, whereby the tensile strength is above 0.1 MPa.

20 The tensile strength increases approximately linearly with compaction pressure for empty PCMs. For drug-and-lipid PCMs, a constant tensile strength is obtained for pressures above 50 MPa. The increased tensile strength at low pressures of drug-and-lipid PCMs is probably due to the high ductility of the lipid mixture. That a lipid, added before compression by a melt method, may increase the tensile strength of tablets has

25 been shown for stearic acid. The constant tensile strength at compaction pressures above 50 MPa could be due to the fact that no further deformation of the lipid is possible and that bonds have formed through all lipid material in the tablet. Some adherence of lipid material to the punch faces support the idea/suspicion that bonds may form due to partial melting or advanced diffusion during compaction. The assumption that bonds may

30 have been formed is also supported by the low melting point of the lipids: 49.5°C for cetanol and 50 - 62°C for hard paraffin. Another explanation for the constant tensile

strength above 50 MPa could be the fact that increased elastic expansion is cancelling out the effect of an increased volume reduction. The lipids appear to act as lubricants. It is not absolutely necessary to add magnesium stearate for the tablets to be ejected from the die. However, an antiadhesion agent may be needed in some instances.

5

### Friability

For the purposes of this invention the friability of a compact member of the invention is defined as the amount of material attrited in a friabilator according to the procedure described below.

10

The friability of the tablets was measured in a friabilator model TA3 (Erweka Apparatebau, Germany). A pre-weighed sample of 10 tablets was rotated for 100 turns at a speed of 25 rpm and the amount of attrited material was determined gravimetrically. The friability expressed as a percentage was then calculated, and shown in Table 2b.

15

TABLE 2B

Friability values for pellets compressed at 12 and 200 MPa, respectively, with and without some additives.

Additives	Friability (%)	
	Compressed at 12 MPa	Compressed at 200 MPa
No additives	2.1	0.27
1% magnesium stearate	8.0	0.30
5% talc	14	0.09
25 5% colloidal silicon dioxide	100 <sup>1</sup>	0.38
5% colloidal silicon dioxide and 1% magnesium stearate	100 <sup>1</sup>	0.14

30

<sup>1</sup> All tablet fragments were smaller than a half tablet after friability test

As can be seen from Table 2b, all tablets compressed at 200 MPa exhibit friability values well below 0.5 %, and even at 12 MPa tablets without any additives exhibit friabilities of no more than 2.1 %. For industrial applications and handling, it is desirable that the friability is less than 1 %, although for certain applications higher friabilities may be acceptable.

#### Friction Properties

For evaluation of the friction, PCMs and mixtures of PCMs with additives was tableted in the single punch press at 12 and 200 MPa ( $\pm 10\%$ ) with automatic feeding and at a rate of approx. 37 tablets/minute. At least 25 tablets were compressed until constant ejection forces were obtained. The maximum upper and lower punch pressures and the ejection forces were then recorded for 10 tablets. The mean height of the tablets were measured after compression. The difference between maximum upper and lower punch pressures per tablet area in contact with the die ( $FD/A$ ) and the ejection force per tablet area in contact with the die ( $EjF/A$ ) were then calculated. These have been suggested as the most useful parameters for the study of friction during compaction. The height of the tablets after ejection was used as an estimate of height of the tablet in the die.

Table 3 shows the results of the evaluation of friction characteristics for different formulations.

TABLE 3

Friction characteristics and observed adhesion for pellets compressed at 12 and 200 MPa, respectively, with and without some additives.

5	Additives	EjF/A (kN/cm <sup>2</sup> )		FD/A (kN/cm <sup>2</sup> )		Observed adhesion (severe/ moderate/ no)
		Compressed at 12 MPa	Compressed at 200 MPa	Compressed at 12 MPa	Compressed at 200 MPa	
10	No additives	0.068 <sup>1</sup>	0.098 <sup>1</sup>	0.101	0.04	severe
	1 % magnesium stearate	0.047 <sup>1</sup>	0.098 <sup>1</sup>	0.095	0.221	moderate
	5 % talc	0.068 <sup>1</sup>	0.080 <sup>1</sup>	0.106	0.304	no
	5 % colloidal silicon dioxide	0.297	0.313	0.280	0.712	no
15	5 % colloidal silicon dioxide and 1 % magnesium stearate	0.137	0.153	0.192	0.638	no

20 <sup>1</sup> The ejection forces were not significantly distinguishable from the background interference

#### Disintegration

25 The disintegration time in deionized water was measured in an Erweka ZT 3 (Erweka Apparatebau, Germany) according to the USP method with discs.

The *in-vitro* drug release rates were determined according to USP method II (paddle) in deionized water, at 37°C with spectrophotometric detection. The stirring speed was 200 rpm. The USP method II (paddle) was used since preliminary trials showed that the tablets did not disintegrate if USP method I (basket) was used. However, in order to study the effect of tablet disintegration on drug release some tests using the basket method at 100 rpm were performed. One tablet or approximately 360 mg

pellets were added to each vessel with 900 ml water. This amount was chosen in order to maintain sink condition during the experiment.

Mean disintegration times were measured (Table 2c and Fig. 2), and was shown to be affected by compaction pressure. Thus, they vary between 8 and 120 minutes for  
 5 PCMs without additives and between 6 and 65 minutes for PCMs with additives such as talc, magnesium stearate and/or colloidal silicon dioxide.

TABLE 2C

Disintegration times for pellets compressed at 12 and 200 MPa, respectively,  
 10 with and without some additives.

Additives	Mean disintegration times (min)	
	Compressed at 12 MPa	Compressed at 200 MPa
15 No additives	8	34
1 % magnesium stearate	9	65
5 % talc	6	19
5 % colloidal silicon		
20 dioxide	9	29
5 % colloidal silicon dioxide and 1 % magnesium stearate	7	25

25 From a medical point of view it is desirable that tablets exhibit disintegration times of less than about 240 minutes, and thus the tablets are well suited for their intended purpose. A maximum was observed at 75 MPa, and at higher and lower compaction pressures respectively, disintegration times were shorter. The decrease of  
 disintegration time at compaction pressures above 75 MPa may be due to the cellulose  
 30 fibres from different pellets getting into closer contact at higher pressures. Hence, more strain is caused by their swelling. Tablets made from unloaded PCMs disintegrated

within less than 3 seconds irrespective of compaction pressure, demonstrating the good disintegrating effect of PCMs. Some small agglomerates of approximately 2-5 pellets could be observed also after disintegration of the tablets for drug-and-lipid PCMs but not for unloaded PCMs.

5       The tablets did not disintegrate when subjected to 100 rpm in the USP apparatus I (basket) as they did in the USP apparatus II (paddle) at 200 rpm (USP method II at 100 rpm caused a partial disintegration). After having been subjected to the basket method for 16 hours the tablets were still coherent although soft and swollen. The swollen tablets disintegrated immediately when gently pressed between the thumb and the index  
10   finger, indicating that *in-vivo* disintegration is probable.

          Interestingly, there was no difference in drug release rate between the two different methods, indicating that the drug release is independent of tablet disintegration. The effect on release rate of compaction pressure and thus disintegration time, is shown in Fig. 4, by comparing the release rates using the two methods USP I (basket) at 100 rpm,  
15   and USP II (paddle) at 200 rpm. In Fig. 4 circles represent tablets compressed at 12 MPa and tested in USP apparatus II (filled circles), and the same tablets tested in USP apparatus I (empty circles), respectively. Squares represent tablets compressed at 200 MPa and tested in USP apparatus II (filled) and USP apparatus I (empty), respectively.

          Without wishing to be bound by any theory, it is believed that the reason for this  
20   may be that pores are rapidly formed between the pellets when the cellulose swells and that the transport in these pores is so rapid that only the diffusion in the pellets will control the release rate. The bonds keeping the swollen tablet coherent may be working over a surface area which is negligible compared to the exposed surface area of the pellets. Hence, the breaking of the bonds does not influence the drug release rate.  
25   However, there may still be bonds over larger surface areas, forming small agglomerates of pellets. These bonds may influence the release rate but they are not necessarily broken during the disintegration of the tablet but may remain unchanged throughout the dissolution process.



### Drug Release

The drug release from tablets compacted at 12 MPa was faster than from uncom-  
pressed pellets. The increase in release rate at 20 MPa was less and at 35 MPa the  
release was slower than for uncompact pellets. Further increase in the compaction  
5 pressure increased the release rate only to a small extent. This is shown in Fig. 5  
wherein release rates for tablets compressed at various pressures are shown as a function  
of time. The tests were performed using the USP II method at 200 rpm. In Fig. 5, empty  
circles and empty triangles represent tablets compressed at 12 MPa and 20 MPa, respec-  
tively. Empty squares and filled squares represent tablets compressed at 35 MPa and  
10 100 MPa, respectively. Filled circles and filled triangles represent tablets compressed at  
200 MPa and uncompressed pellets, respectively.

Again without wishing to be bound by any specific theory, it is possible that the  
increase in release rate at low pressures may be due to some lipid being squeezed out of  
the PCMs during compression, increasing the porosity and surface area of the pellets. At  
15 higher compaction pressures, lipid may be squeezed back into the pores of the PCMs. In  
this process, some of the drug is redistributed and less drug may be exposed at the surfa-  
ces of the PCMs. It has been shown that the incorporation process may cause a higher  
drug concentration close to the surface of the PCMs than in the centre of the matrices. It  
is also possible that higher compaction pressures may increase the number of small ag-  
20 lomerates of spheres, which do not deagglomerate upon tablet disintegration. Conse-  
quently, the surface area of the matrices will decrease.

For pure pellets or mixtures with magnesium stearate or talc, the lower punch  
forces detected during the ejection were not significantly different from the background  
reference (Table 3). When colloidal silicon dioxide was added the ejection force (EjF)  
25 increased. An addition of 1 % magnesium stearate to the silicon dioxide mixture  
decreased the ejection force somewhat. As expected, FD/A values were low for pure  
pellets compacted at both 12 and 200 MPa. Addition of magnesium stearate or talc did  
not increase FD/A. Colloidal silicon dioxide, on the other hand, increased FD/A. This  
indicates that no lubricant is needed for the tableting of extended release pellets prepa-  
30 red by the incorporation of lipid release modifiers into PCMs. However, since some  
adherence to punch faces was seen, addition of an antiadherent may be necessary. If so,

talc gives better friction properties than colloidal silicon dioxide when added at the same concentration.

Addition of excipients (magnesium stearate, talc and/or colloidal silicon dioxide) decreased the tensile strength of the tablets compacted at 12 MPa (Table 2a).

5 For tablets compressed at 200 MPa the effect of additions of excipients on tensile strength was small. It is contemplated, without knowing the exact mechanism, that the lack of effect of excipients on tensile strength at higher compaction pressure may be due to the high ductility of the lipids, which means that the lipids could flow around the excipient particles and create bonds around them. It is well known that a  
10 high tendency of a substance to fragment during compaction will counteract the tensile strength, lowering effect of magnesium stearate. However, it seems reasonable that extreme ductility may have the same effect. Extreme deformation of a substance will lead to redistribution of the magnesium stearate covering its surfaces.

The effect on disintegration times of the added excipients was low at 12 MPa. At  
15 200 MPa the disintegration time was increased by magnesium stearate and decreased by talc. The increase in disintegration time, when magnesium stearate is added, is expected due to the hydrophobic nature of this substance while an explanation for the decrease seen when talc is added is less obvious.

The friability of tablets with no additives and compressed at 12 MPa was 2.1%.  
20 Addition of excipients (especially colloidal silicon dioxide) increased the friability considerably. At 200 MPa the friability of pure pellets and all investigated mixtures was below 0.5 % which indicates a sufficient tablet strength for industrial handling.

Addition of magnesium stearate and talc did not affect the release rate from tablets compressed at 12 MPa. A small increase in the release rate was seen when  
25 colloidal silicon dioxide was added. At 200 MPa all additions gave an increase of the release rate. The increase in the release rate was highest for 5 % colloidal silicon dioxide and 5 % colloidal silicon dioxide + 1 % magnesium stearate. The increase was smaller when 1 % magnesium stearate was added. For all three mixtures containing silicon  
30 dioxide and/or magnesium stearate, the release rate was faster than from the uncompressed pellets. The release from tablets without additives was slower than from uncompressed pellets.

Surprisingly, the release rate from tablets containing an active drug (paracetamol), with and without added talc (5 % w/w) was approximately the same as from uncompressed pellets. This effect is shown in Fig. 6, wherein filled circles represent tablets without talc and compressed at 200 MPa. Empty triangles represent tablets with talc and compressed at 200 MPa. Crosses represent uncompressed pellets without talc. This suggests that it is possible to produce extended release multiple-unit tablets from drug-and-lipid PCMs with only a small amount of additives.

The higher release rate in the presence of additives may be due to the added substances forming a coating layer around the pellets. This coating layer may then either prevent the formation of non-disintegrating agglomerates or influence the redistribution of drug particles during compression. Another possible explanation for the increased release rate is that hydrophilic additives are pressed into the matrix pellets thereby increasing their hydrophilicity. This may be a possible mechanism for silicon dioxide but seems less probable for talc and magnesium stearate.

Thus, in accordance with the invention, extended release matrix pellets prepared by incorporation of release modifiers, especially lipids, into PCMs can be compacted into disintegrating tablets without the addition of any excipients. The release rate is increasing at low compaction pressures and decreasing at higher pressures. By addition of 5 % talc it is possible to achieve the same release profile from tablets compacted at 200 MPa as from uncompacted pellets. The disintegration times appear to be relatively long at higher pressures but on the other hand, drug release appears to be independent of tablet disintegration. The pellets seem to be self lubricating although an addition of antiadherent may be necessary.

CLAIMS

1. A compact member comprising a plurality of porous cellulose matrices (PCMs),  
and providing extended release of an active compound contained therein, c h a r a c t e -  
5 r i z e d in that
- a) said active compound and a release-modifying agent is located in the pores of  
said PCMs;
  - b) the friability of the compact member is less than 2.1%, suitably less than 1%,  
preferably less than 0.5%; and
  - 10 c) the disintegration time *in-vitro* (measured with the USP method with discs) of  
said compact member is less than about 240 minutes, suitably less than 90  
minutes, preferably less than 60 minutes.
2. The compact member according to claim 1, wherein the radial tensile strength of  
15 the compact member is higher than about 0.1 MPa, preferably higher than 0.5 MPa.
3. The compact member according to claim 1 or 2, wherein said release-modifying  
agent has a melting point in the range of from about 10°C up to about 200°C, preferably  
from 30°C up to 100°C.
- 20 4. The compact member according to any preceding claim, wherein said release-  
modifying agent is a lipid.
5. The compact member according to claim 4, wherein said lipid is selected from  
25 the group consisting of fatty acids, e.g. stearic acid, long chain alcohols, e.g. cetostearyl  
alcohol, naturally occurring and synthetic waxes, glyceryl esters of fatty acids, e.g.  
glyceryl monostearate, glyceryl distearate, or glyceryl tristearate, aliphatic hydro-  
carbons, e.g. hard paraffin, polyglycerol esters of fatty acids, and any mixture thereof.
- 30 6. The compact member according to any preceding claim, further comprising up to  
about 10 % by weight of talc, preferably up to 5 %.

7. The compact member according to any preceding claim, further comprising up to about 5 % by weight, suitably up to about 1 % by weight, of a lubricant, e.g. magnesium stearate.

5

8. The compact member according to any preceding claim, comprising up to about 50 % by weight of said active compound, preferably up to 2.5 %.

9. The compact member according to any preceding claim, wherein said active  
10 compound is a drug.

10. The compact member according to claim 9, wherein said drug is hydrophilic.

11. The compact member according to claim 9 or 10, wherein said drug has a  
15 biological half-life of less than about 20 hours.

12. The compact member according to any preceding claim, comprising a tablet suitable for oral administration.

20 13. The compact member according to any of claims 1-8, wherein said active compound is selected from the group consisting of fertilizers, herbicides and pesticides.

14. A method of manufacturing a compact member providing extended release of an active compound, the method comprising

- 25 a) exposing a plurality of porous cellulose matrices (PCMs) to an active compound and a release-modifying agent, in optional sequence or mixture, for a time sufficient for said active compound and release-modifying agent to fill the pores in said PCMs to a preselected level; and
- b) compacting said PCMs comprising said active compound and release-modifying  
30 agent, to a desired shape.

15. The method according to claim 14, wherein the pressure in the compacting step is less than about 500 MPa, preferably in the range of from 10 up to 200 MPa.
16. The method according to claim 14 or 15, wherein said release-modifying agent is  
5 a lipid.
17. The method according to claim 16, wherein said lipid is selected from the group consisting of fatty acids, e.g. stearic acid, long chain alcohols, e.g. cetostearyl alcohol, naturally occurring and synthetic waxes, glyceryl esters of fatty acids, e.g. glyceryl  
10 monostearate, glyceryl distearate, or glyceryl tristearate, aliphatic hydrocarbons, e.g. hard paraffin, polyglycerol esters of fatty acids, and any mixture thereof.
18. The method according to any of claims 14-17, wherein up to about 10 % by weight, preferably up to 5 % by weight of talc is incorporated in said compact member.  
15
19. The method according to any of claims 14-18, wherein up to about 5 % by weight, suitably up to about 1 % by weight, of a lubricant, e.g. magnesium stearate, is added to the preparation before compaction.
20. Use of a compact member according to any of claims 1-13 for administration of  
20 a drug.



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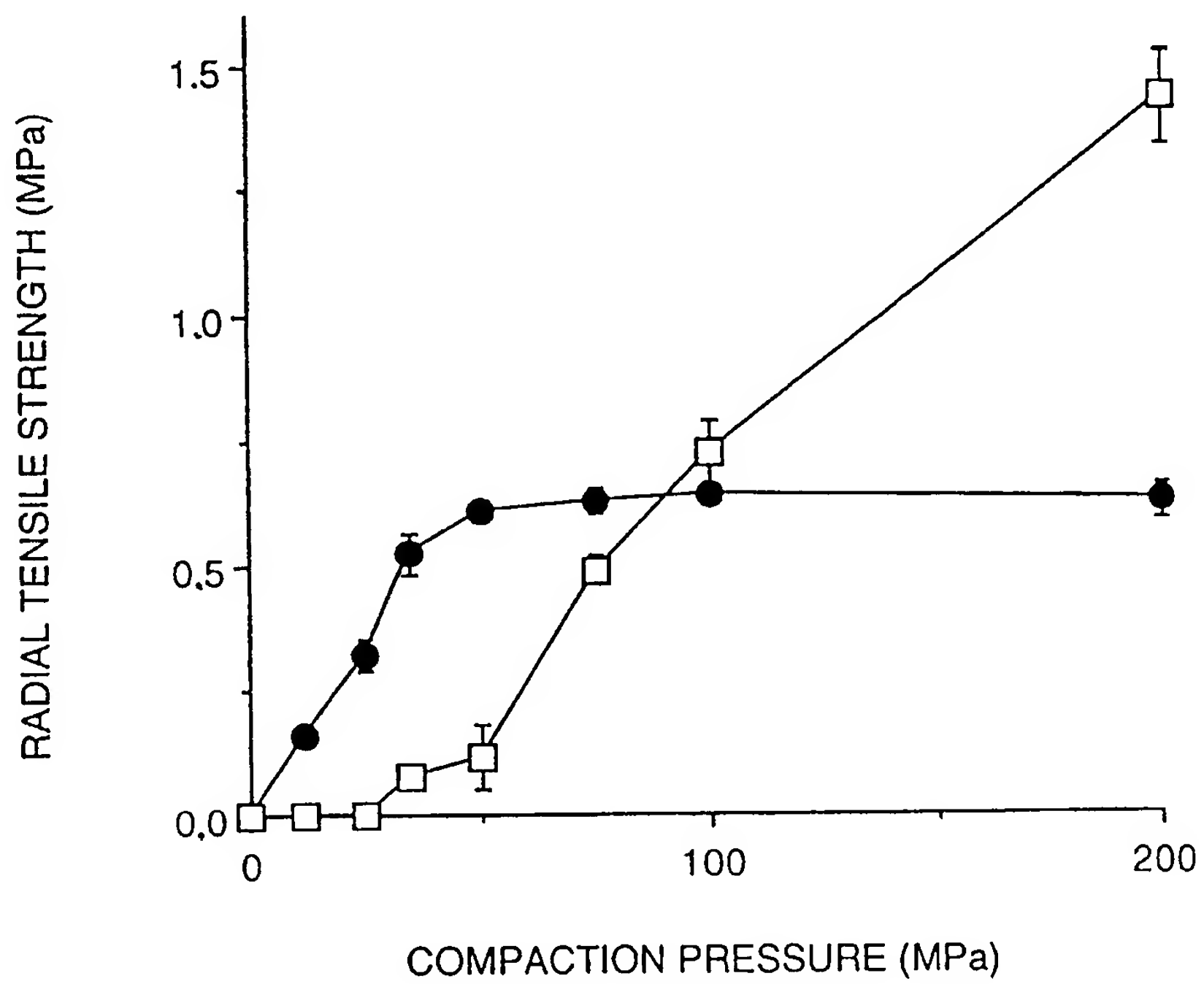


Fig. 1

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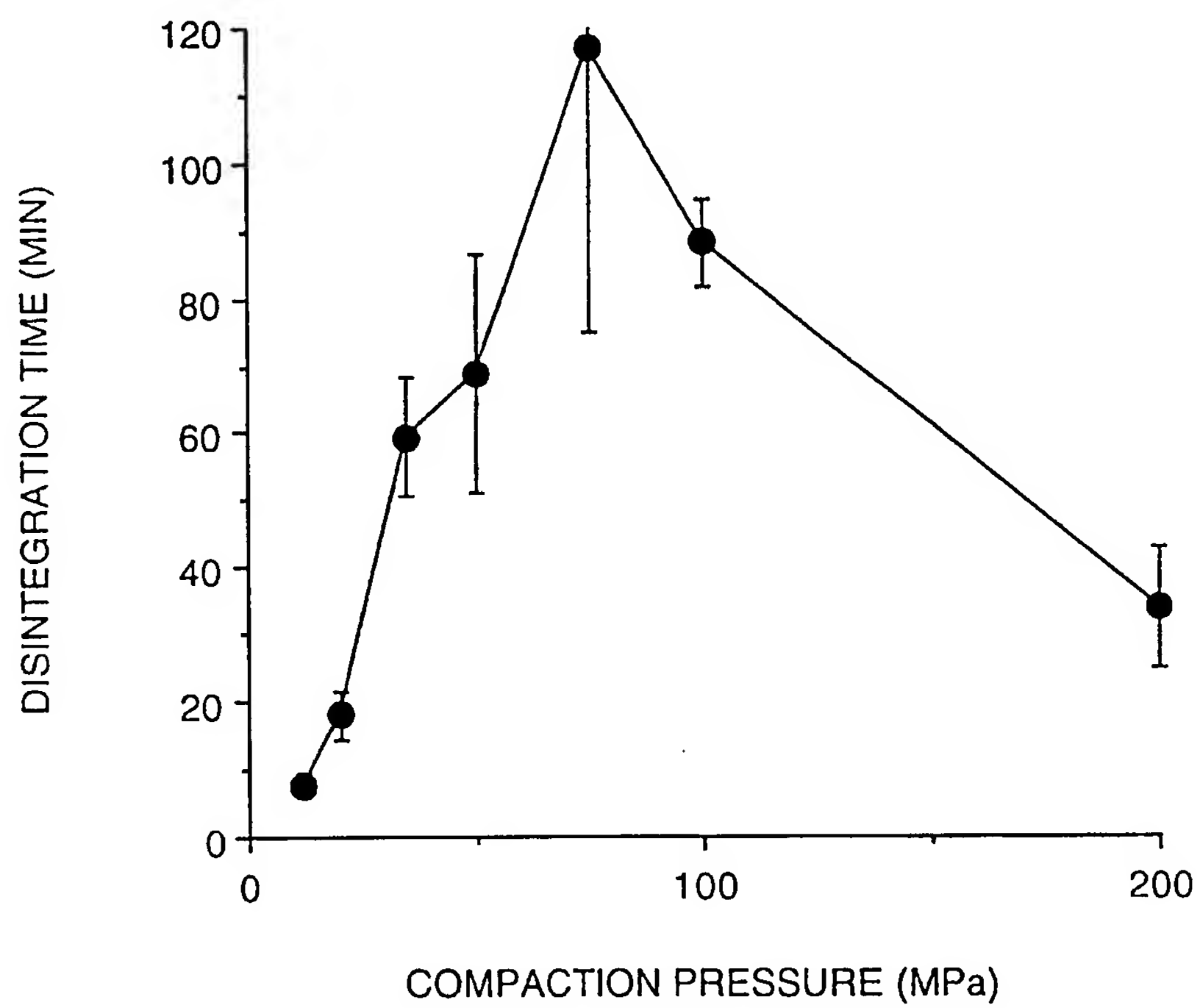


Fig. 2

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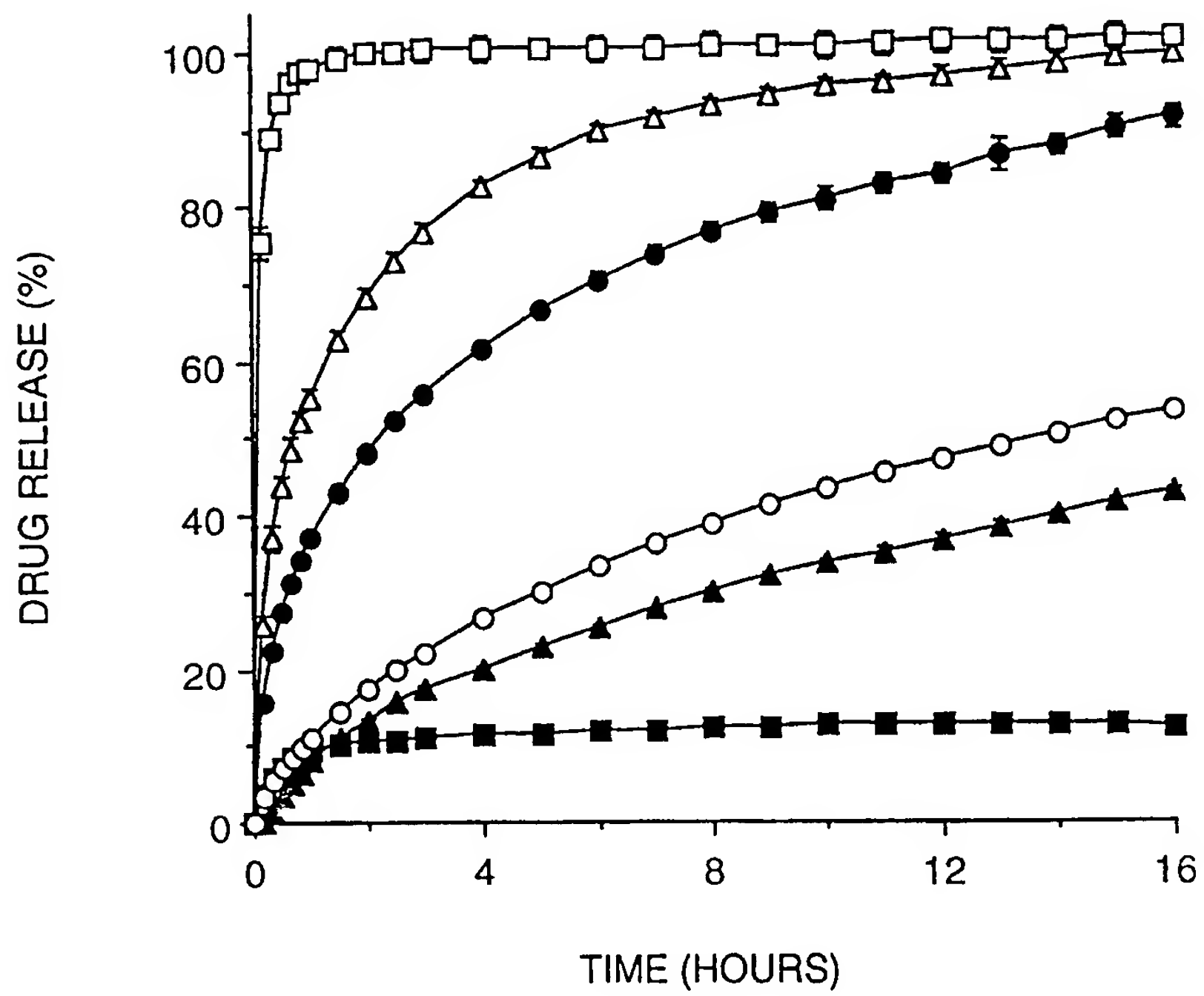


Fig. 3

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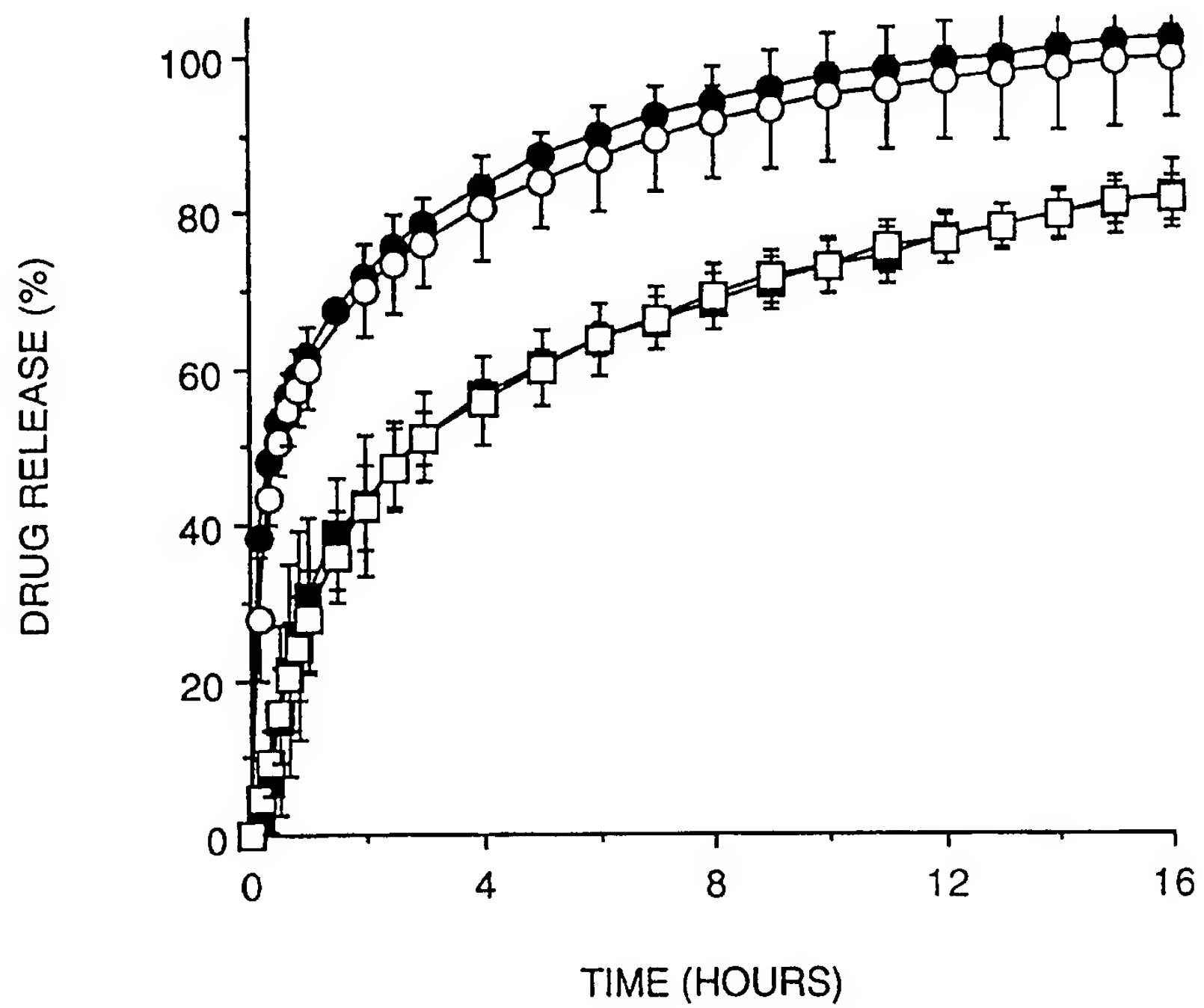


Fig. 4

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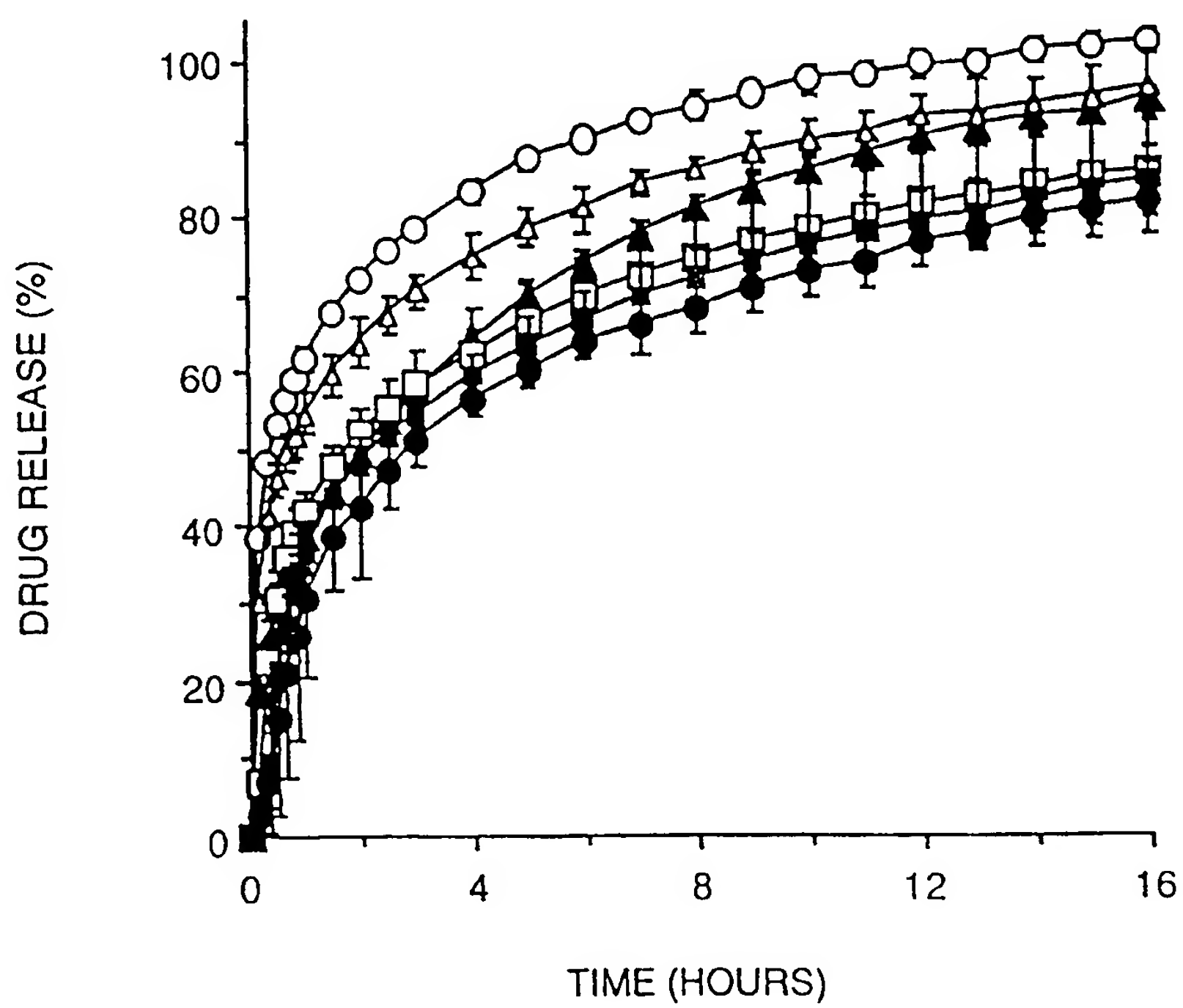


Fig. 5

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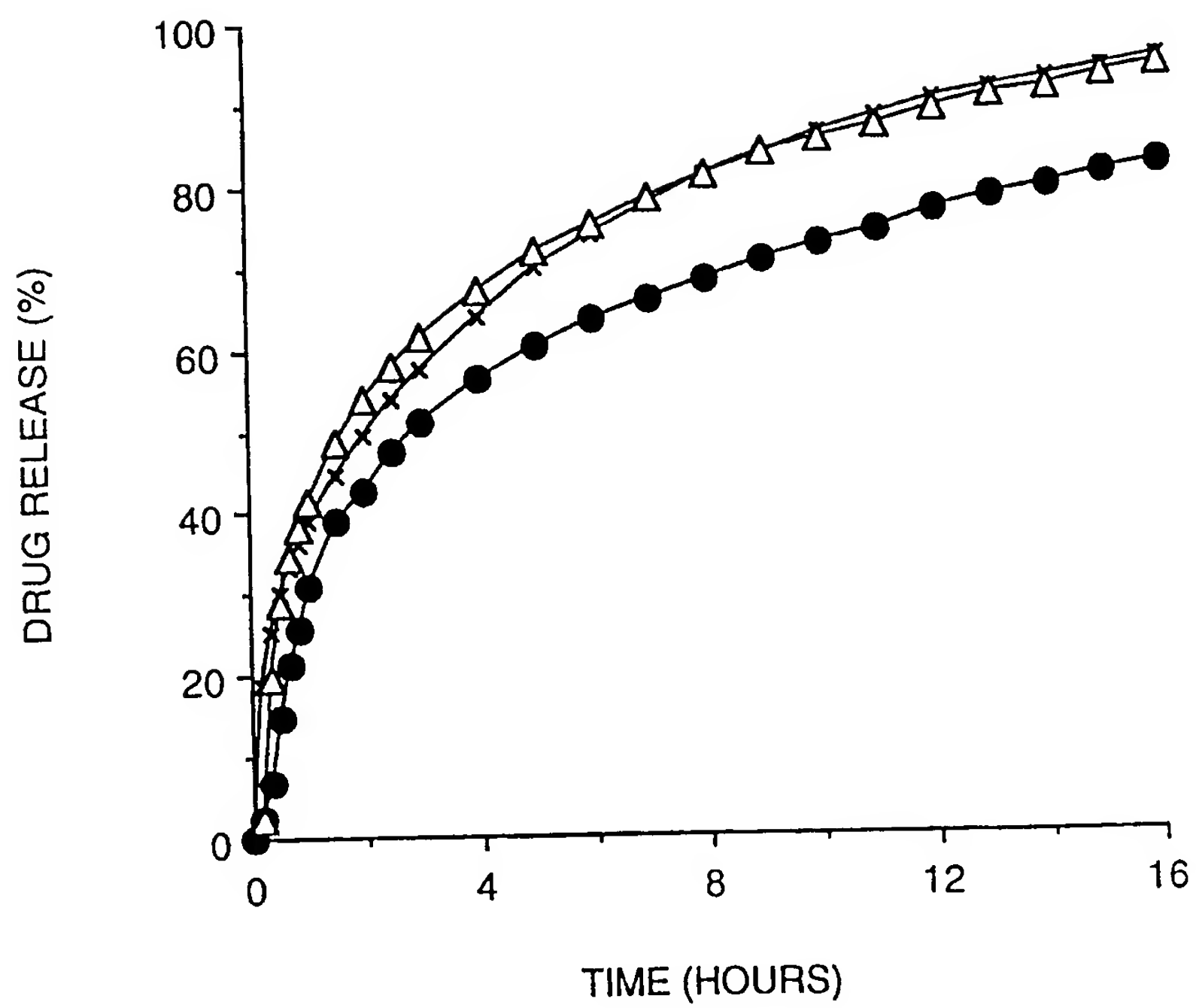


Fig. 6



# INTERNATIONAL SEARCH REPORT

International application No.

PCT/SE 97/01901

## A. CLASSIFICATION OF SUBJECT MATTER

IPC6: A61K 9/16, A61K 9/20

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC6: A61K

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

SE,DK,FI,NO classes as above

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EMBASE, WPI, USPATFULL, CAPLUS, MEDLINE

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	International Journal of Pharmaceutics, Volume 100, 1993, Ricardo Davidson et al, "Porous cellulose matrices - a novel excipient for the formulation of solid dosage forms", page 49 - page 54, page 53, column 1, line 5-23; page 54, column 2, line 1-12	1-3,6-15, 18-20
A	--	4-5,16-17
Y	WO 9119483 A1 (ADVANCED POLYMER SYSTEMS, INC.), 26 December 1991 (26.12.91), page 4, line 1 - line 18; page 12, line 24 - line 37	1-3,6-15, 18-20
A	WO 9423703 A1 (KABI PHARMACIA AB), 27 October 1994 (27.10.94)	1-20

☒ Further documents are listed in the continuation of Box C.

☒ See patent family annex.

\* Special categories of cited documents:

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"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

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"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

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Date of the actual completion of the international search

24 February 1998

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Date of mailing of the international search report

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# INTERNATIONAL SEARCH REPORT

International application No.  
PCT/SE 97/01901

## C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	<p>WO 9118590 A1 (KABI PHARMACIA AB), 12 December 1991 (12.12.91)</p> <p style="text-align: center;">-- -----</p>	1-20

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Information on patent family members

03/02/98

International application No.

PCT/SE 97/01901

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